RESEARCH ARTICLE

Influence of cervical and middle preparation on the cyclic fatigue resistance of Logic 25.06 rotary instruments: Replica study

Ana L. C. Binda¹, Ana G. Limoeiro², Virgilio Braga¹, Michel Klymus², Luanna S. S. Vasconcellos¹, Augusto L. Andrade¹, Wayne M. Nascimento¹, Adriana J. Soares³, Marilia F. V. Marceliano-Alves⁴⁻⁶, Marcos Frozoni¹

¹Departamento de Endodontia, Faculdade São Leopoldo Mandic, Campinas, SP, Brasil

²Departamento de Dentística, Endodontia e Materiais Odontológicos, Faculdade de Odontologia de Bauru – USP, Bauru, SP, Brasil

³Departamento de Endodontia, Faculdade de Odontologia de Piracicaba – UNICAMP, Piracicaba, SP, Brasil

⁴Universidade Iguaçu, Programa de Pós-Graduação em Odontologia, Nova Iguaçu, Rio de Janeiro, Brasil

⁵Centro Universitário Maurício de Nassau (UNINASSAU), Rio de Janeiro, Brasil

⁶Department of Dental Research Cell, Dr. D. Y. Patil Vidyapeeth, Pune 411018, India



PUBLISHED
31 December 2025

CITATION

Binda, A., L., C., Limoeiro, A., G., et al. Influence of cervical and middle preparation on the cyclic fatigue resistance of Logic 25.06 rotary instruments: Replica study, [online] 13(12).

https://doi.org/10.18103/mra.v13i12. 7115

COPYRIGHT

© 2025 European Society of Medicine. This is an open-access article distributed under the terms of the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original author and source are credited.

DOI

https://doi.org/10.18103/mra.v13i12. 7115

ISSN

2375-1924

ABSTRACT

Introduction: The aim of this study was to evaluate the influence of cervical and middle preparation on resistance to dynamic cyclic fatigue during instrumentation of mandibular molar replicas with Logic 25/.06 instruments.

Materials and Methods: Forty mandibular molar replicas were printed with 16 µm resolution from a tooth file scanned by microcomputed tomography. For the fatigue test, 40 new Logic 25/.06 nickel-titanium instruments (Bassi Endo, Belo Horizonte, Brazil) were used for mechanical preparation of the mesiobuccal canal and subjected to the dynamic cyclic fatigue test in an artificial curved metal canal with a bending angle of 45° and a bending radius of 6.6 mm. During the dynamic cyclic fatigue test, the time to fracture of the file was recorded and the number of cycles to fracture was calculated. The surfaces of the fragments were evaluated using scanning electron microscopy to verify the length of the fragment and the type of fracture that occurred. Data on time to fracture, number of cycles to fracture, and length of the fractured fragment were collected and statistically analyzed using the t-test or Mann-Whitney test with a significance level of 5%.

Results: There were no statistically significant differences between the groups with or without preparation of the cervical and middle third in relation to time to fracture (p = 0.561), number of cycles to fracture (p = 0.508), and length of the fractured fragment (p = 0.417).

Conclusion: Preparation of the cervical and middle thirds did not increase the resistance to fracture due to cyclic fatigue of the instruments tested.

Keywords: Cyclic fatigue; Instrumentation; Root canal preparation.

Introduction

Endodontic treatment is essential to preserve health and repair periradicular tissues¹. Its phases involve root canal preparation, including cleaning and shaping the dentin walls, using irrigation containing an antimicrobial chemical substance². Mechanical instrumentation contributes to accurate canal preparation, effective removal of bacterial contamination, facilitation of chemical debridement, and creation of the space necessary for subsequent root canal filling^{2,3}.

The introduction of nickel-titanium (NiTi) instruments in endodontics represented an evolution in biomechanical preparation due to the physical properties of the alloy, giving them remarkable flexibility⁴⁻⁶. Furthermore, it provided several advantages, such as reduced preparation time, cutting efficiency, and the ability to centralize the root canal when compared to manual stainless-steel instruments⁷.

Despite these benefits, the preparation of curved canals presents challenges, such as risks of instrument fracture due to constant alternations of forces and tensions during preparation, which can lead to material fatigue^{8,9}. Fracture of NiTi instruments can occur due to torsion or cyclic fatigue^{5,10}. Torsional fracture occurs when the end or another portion of the instrument gets caught in the canal and the handle continues to rotate ^{11,12} Fracture of the instrument occurs when the torque exceeds the elastic limit of the metal⁵.

One instrument that deserves to be highlighted are the Logic instruments (Bassi Endo, Belo Horizonte, Brazil). These instruments are found in diameters from #15 to #50, with constant tapers and modified S-shaped cross-sectional designs, variable helical angle with two cutting blades, and clockwise rotation^{13,14}. Their manufacturing process is based on the heat treatment of CM-Wire.

Performing coronal preflaring has the potential to extend the cyclic fatigue life of instruments¹⁰ Therefore, carrying out this procedure beforehand

can provide greater safety when using rotating instruments. To date, there are no data available on the influence of cervical preparation prior to instrumentation with the Logic 25/.06 system.

Thus, the objective of this study was to evaluate whether cervical and middle preparation can increase the resistance to cyclic fracture of the Logic 25/.06 rotary system in an artificial canal simulating curvature in the apical third. The null hypothesis tested was that there would be no difference in resistance to cyclic fatigue with or without cervical and middle canal preparation.

Materials and Methods

SAMPLE SELECTION

The present study was approved by the local ethics and research committee (CAAE: 76207123.0.0000.5374). A total sample of 40 new heat-treated NiTi instruments (Logic 25/.06, Bassi Easy) 25 mm long were used in the study. All instruments were inspected using stereomicroscope (Carl Zeiss, LLC, Oberkochen, Germany) at 20x magnification to observe the presence of deformities or defects. No defects were detected. The forty selected instruments were used in the two experimental phases of this study: first, the instruments were used during the preparation of root canals from 3D-printed replicas of a mandibular molar previously scanned by microcomputed tomography. Next. the instruments were subjected to the cyclic fatigue test.

3D PRINTING OF MANDIBULAR MOLAR REPLICAS AND PREPARATION OF THE STUDY MODEL

An extracted human mandibular molar was selected, with Vertucci type IV mesial canals. The tooth had no previous endodontic treatment, no fractures or resorptions, a moderate curvature angle (10° to 20°), and an anatomical diameter of the foramen compatible with a NiTi #15/.02 C-Pilot instrument (VDW, Munich, Germany). The tooth

was immersed in 5.25% sodium hypochlorite (NaOCI) for one hour for disinfection, and its external surface was cleaned using periodontal curettes.

Coronal access was performed with high-speed drills (1014HL and 1558, KG Sorensen Indústria e Comércio Ltda., São Paulo, Brazil), under constant irrigation, and patency was performed with C-Pilot #10 and #15 hand files (VDW). The coronal portion of the tooth was partially removed with a diamond disc (KG Sorensen) at low speed until a length of 18 mm was obtained: 4 mm for the apical third, 4 mm for the middle third, 4 mm for the cervical third, and 6 mm for the coronal portion.

The specimen was scanned using a SkyScan 1174 (Bruker micro-CT, Kontich, Belgium) using voltage parameters of 100 kV and 100 μ A current with a resolution of 26.80 μ m; 360° rotation, copper and aluminum filter, 0.6° rotation, and 30-minute exposure. The images were reconstructed using the NRecon 16.9.16 program (Bruker micro-CT) and converted into Bitmap images using the following parameters: Smothing of 5, Ring artefact correction of 6, and Beam Hardening of 30%.

The data acquired after micro-CT were exported into STL files using the CTan 1.14.4.1 program (Bruker micro-CT) and 20 replicas of the lower molar were printed on a three-dimensional (3D) printer (Halot One, Creality 3D, Shenzhen, China), using a high-precision resin (3D Dental Align, 3D Cure, Betim, Brazil).

ERGONOMIC WORKING POSITION

To simulate the periodontal ligament and alveolar bone during canal preparation, the roots of the 3D replicas were wrapped with Teflon tape and placed inside heavy condensation silicone blocks (Zetaplus, Ahermack, Rovigo, Italy). This setup, comprising the replicas and the impression material, was placed on a dental mannequin to simulate clinical conditions.

The 3D replicas of the teeth were isolated using a rubber dam (Madeitex, São José dos Campos,

Brazil). The dental simulator mannequin was fixed to the dental chair, positioning the lower occlusal plane perpendicular to the ground to simulate the patient's position, with the operator situated between the noon and nine o'clock positions.

ROOT CANAL PREPARATION

The canal length (CL) was measured clinically by the direct visual method using a microscope (Decius, DF Vasconcelos Valença, Brazil) at 30x magnification. A 10/.02 C-Pilot manual file (VDW) was introduced into the canal, passing 1 mm beyond the foramen, and then retracted until the tip of the file reached the edge of the apical foramen. The working length (WL) standardized to be equal to the CL. Subsequently, tooth replicas and endodontic instruments were randomly distributed into two experimental groups (n = 20):

GROUP WITHOUT CERVICAL AND MIDDLE PREPARATION:

The 10/.02 and 15/.02 C-Pilot hand files (VDW) were introduced into the mesiobuccal canal throughout the WL (18 mm). The Logic 25/.06 instrument was activated in a rotational movement coupled to the iRoot Pro motor (Bassi/Easy). The preparation of the root canals was carried out in the crown-down direction, in an in-and-out movement with approximately 3 mm of amplitude ¹⁵. After every movement, the instrument was cleaned with gauze and the canal was irrigated with 2.5 mL of 5.25% NaOCI.

GROUP WITH CERVICAL AND MIDDLE PREPARATION:

This group followed the same initial protocol as the group without cervical and middle preparation. However, after achieving patency with manual files, the 17/.08 Orifice Shaper file (Mklife, Porto Alegre, Brazil) was used for preflaring. The Logic 25/.06 instrument performed the mechanical preparation in the same way as described for the group without cervical and middle preparation.

A final irrigation with 2.5 mL of saline and 1 mL of 17% EDTA was performed on all replicas. Each Logic 25/.06 instrument was used only once to instrument the mesiobuccal canals of each 3D replica. All canal preparations were performed by a single previously calibrated Endodontist.

CYCLIC FATIGUE TEST

The instruments previously employed underwent testing to assess their resistance to dynamic cyclic fatigue fracture. These tests utilized an artificial root canal, as described by Al-Nasrawi et al. ¹⁶, with the following specifications: a straight cervical segment measuring 6.5 mm (from the canal entrance to the curvature's initiation), a curved section with a length of 3.0 mm, a curvature radius of 4.0 mm, an angular curvature of 45°; and a straight apical segment measuring 2.5 mm (from the curvature's end to the canal apex), featuring diameters of 1.0 mm within the cervical 5 mm, 0.7 mm in the intermediate 4 mm, and 0.5 mm within the apical 3 mm.

The tests were conducted dynamically, with the mechanical movement system being powered by a SAVOX SC-12 56T69 motor (Savox All Rights Reserved, Taichung, Taiwan), inducing back-and-forth motion of the mechanical system. This motion was guided by a linear guide under the control of an electronic processor, regulating the speed and range of the instrument's movements to replicate the axial motion seen in endodontic procedures.

The instruments were attached to the VDW Gold motor (Dentsply-Sirona) and inserted into the metal canal to a depth of 12 mm. They were activated using the "ROTATORY" setting at a speed of 900 rpm, with an in-and-out amplitude of 3 mm. These movements were standardized and repeated until fracture occurred. The stainless-steel plate containing the simulated canal was positioned on a heated plate maintained at a controlled temperature of 37°C to closely mimic clinical conditions.

To reduce the friction of the file when in contact with the walls of the artificial canal, a mineral oil (WD 40 Company, Milton Keynes, United Kingdom) was applied inside the canal for lubrication and to prevent a temperature increase ¹⁶. Video recording of the test was performed simultaneously using a smartphone (Poco M5S), from the beginning of the file activation until its fracture. Video analysis was conducted using Microsoft Movie Maker software. The NCF of the instrument was calculated by multiplying the number of rotations per minute (RPM) by the time in seconds and dividing by 60. The same researcher who performed the canal instrumentation also conducted the cyclic fatigue tests. The fractured fragments were measured using a 150 mm digital caliper, with an accuracy of $\pm 0.03 \text{ mm}/0.001.$

SCANNING ELECTRON MICROSCOPY (SEM)

The fractured surface of each instrument subjected to the cyclic fatigue test was evaluated by SEM. The analysis was carried out in a horizontal position to detect whether there was plastic deformation and the fracture pattern among the instruments in each group ¹⁷.

STATISTICAL ANALYSIS

Data were analyzed using Mann-Whitney tests, given the non-normal distribution of the data. The SPSS 23 program (SPSS Inc., Chicago, IL, USA) was used for statistical calculations, setting the significance level at 5%.

Results

There was no significant difference between the groups without and with cervical and middle preparation with the Orifice Shaper file in relation to time to fracture (TF) (p = 0.561), NCF (p = 0.508), and the length of the instrument fragment (p = 0.417), as indicated in table.

Table 1: Means and standard deviations of time and number of cycles to fracture (NCF) and fragment length of Easy Logic 25/.06 files, used in canals without and with cervical and middle preparation.

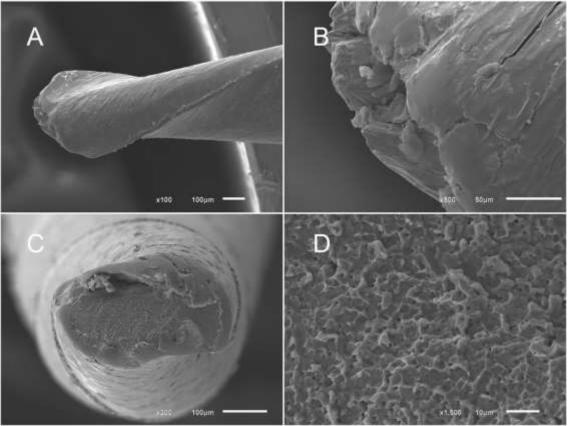
Pre-flaring	Time (seconds)	NCF	Length(mm)
Absent	166 (73) A	2803 (1325) A	1,4 (0,7) A
Present	149 (54) A	2477 (1039) A	1,4 (0,6) A

Legend: Averages followed by equal letters indicate no statistically significant difference between the groups without and with pre-widening (comparisons within each column).

The SEM evaluation of the fractured surfaces (figures 1 and 2) showed similar and typical characteristics of cyclic fatigue for all instruments tested. The fractured surfaces demonstrated

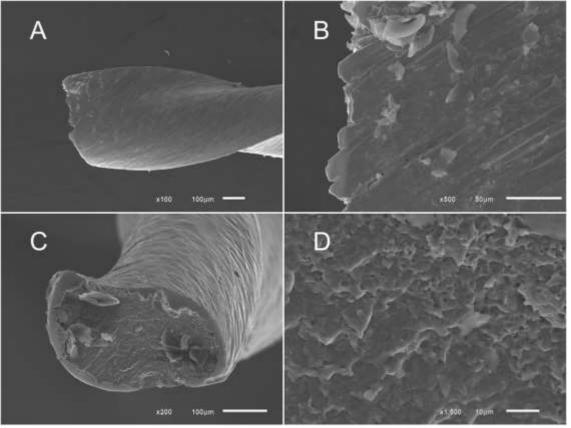
ductile-type characteristics, with areas of crack initiation and zones characteristic of rapid fractures due to overload.

Figure 1: SEM images of an instrument from the group without cervical and middle preparation after the cyclic fatigue test.



Caption: SEM - Scanning Electron Microscopy; A - magnification 100x - 100 μ m; B - magnification 500x - 50 μ m; C - magnification 200x - 100 μ m; D - magnification 1500x - 10 μ m.

Figure 2: SEM images of an instrument from the group with cervical and middle preparation after the cyclic fatigue test.



Caption: SEM - Scanning Electron Microscopy; A - magnification 100x - 100 μ m; B - magnification 500x - 50 μ m; C - magnification 200x - 100 μ m; D - magnification 1500x - 10 μ m.

Discussion

During the chemical-mechanical preparation of the canals, preflaring aims to remove root interferences, ensuring sufficient space for the penetration of mechanical instruments and allowing the free path of the files to the apical third ². However, current evidence is inconclusive and scarce regarding the impact of this additional preparation on the cyclic fatigue resistance of endodontic instruments in rotary movements. The objective of the present study was to investigate whether preflaring can increase the cyclic fatigue resistance of the Logic 25/.06 rotary system. The instruments were used during the preparation of root canals from a replica printed on a 3D printer and subjected to the cyclic fatigue test in an artificial curved canal.

In this study, 3D replicas from a natural tooth scanned using microcomputed tomography were used. This approach aims to overcome the limitations associated with obtaining models from

extracted teeth, such as ethical difficulties and sample standardization issues¹⁸. Previous studies have highlighted the difficulty in standardizing samples as a significant limitation of the methodology, even when using microcomputed tomography on extracted specimens ^{19,20}. Thus, laboratory studies using 3D resin replicas allow control over experimental conditions, ensuring that only the variables of interest are analyzed ¹³.

For the cyclic fatigue test, a device already used in previous studies was employed and proved to be effective for this purpose ^{6,21}. A 45° curvature was adopted ^{16,22}.

Temperature is a variable that can significantly affect the cyclic fatigue resistance of NiTi instruments ^{6,23,24}. La Rosa et al. ²³ found that NiTi files used at room temperature showed greater resistance to cyclic fatigue compared to those used at body temperature. This is due to the nature of the NiTi alloy, characterized by two heat-

dependent crystalline states (martensite and austenite), and the properties of the metal vary in each of these phases. The metal is stiffer in the austenitic phase at temperatures higher than the transformation level, resulting in a decrease in resistance to cyclic fatigue ²³.

In this study, NaOCI was used as an irrigating chemical substance due to its widespread use in endodontic practice and its interaction with the surface of instruments (corrosive properties), which may impact resistance to cyclic fatigue 25. However, Pedullà et al. ²⁶ demonstrated that immersion in NaOCI for 1 or 5 minutes does not significantly reduce the resistance of nickel-titanium instruments to cyclic fatigue. Furthermore, there are no studies in the literature that demonstrate how NaOCI can influence the physical properties of resin models. Moreover, the interplay between dentin and auxiliary chemical substances plays a role the chemical-mechanical critical in instrumentation process, affecting the cutting efficiency of the instrument as highlighted by Tanomaru et al., 21. This interaction's nuances are challenging to replicate accurately in resin models.

Operator experience as an independent variable is one of the most consistent and predictable parameters in instrument separation ²⁷. So, in this study, the tests were conducted by a trained specialist with experience in using the Logic rotary system.

The results of this research revealed that cervical and middle preparation did not interfere with the resistance to dynamic cyclic fatigue of the Logic instruments; therefore, the null hypothesis was accepted. This lack of effect can possibly be attributed to the heat treatment of the CM wire of Logic instruments during their manufacturing process. This treatment is known to produce a better arrangement of the crystal structure, resulting in greater flexibility and greater resistance to cyclic fatigue. Furthermore, this treatment is responsible for stronaly influencing the martensitic/austenitic transformation behavior. allowing a greater percentage of martensitic transformation and the dissipation of the energy necessary for the formation and/or propagation of cracks during cyclic fatigue tests ^{28,29}.

These findings contrast with another study ³⁰ that demonstrated that coronal preflaring increased the cyclic fatigue resistance of the Reciproc and WaveOne instruments. The controversies in these results may be related to different methodologies and different thermal treatments of the alloys. In the present study, the instruments were taken out of the box, used once in resin blocks, and subjected to the cyclic fatigue test. In the study by Maniglia et al., ³⁰ extracted human molars were used, and each file was used repeatedly until fracture occurred.

The ProDesign Logic and ProDesign R instruments tolerated a greater number of cycles to fracture (910.37 and 761.93, respectively) compared to Wave One Gold ¹³. In the present study, the Logic instrument tolerated a greater number of cycles until fracture occurred (2477-2803). The discrepancies between different studies can be explained by differences in root canal curvature, instrument rotation, speeds, and torque. In this study, the speed was 3 times higher than in the study by Menezes et al., ¹³.

The micrographs obtained by SEM revealed a similar pattern in the experimental groups. Both groups exhibited regions with microcracks and ripples, indicative of high stress concentration, suggesting a failure characteristic of cyclic fatigue ³¹. These results contribute to the understanding of the similarity observed in the length of the fractured fragments, as the stressed areas in both groups were formed in a similar manner.

However, it is essential to exercise caution when extrapolating these results to the clinical context, given that the microhardness of resin blocks differs from that of human dentin (25 to 93.3 on the Knoop scale). This difference can compromise the cutting mechanics of the instruments and may not reliably

reproduce the effects of canal instrumentation on the mechanical properties of the instrument. Therefore, future studies should compare the impact of using extracted teeth and 3D prototypes in evaluating the mechanical properties of instruments.

Conclusion

Based on the results obtained in this study and the methodology used, it is concluded that cervical and middle preflaring did not increase the resistance to cyclic fatigue of the instruments tested.

Conflict of Interest:

The authors have no conflicts of interest to declare.

Funding Statement:

No financial disclosure.

References:

1.Santosh SS, Ballal S, Natanasabapathy V. Influence of Minimally Invasive Access Cavity Designs on the Fracture Resistance of Endodontically Treated Mandibular Molars Subjected to Thermocycling and Dynamic Loading. J Endod. 2021;47(9):1496-1500. doi:10.1016/j.joen.2021.06.020

2.Perez R, Neves AA, Belladonna FG, Silva EJNL, Souza EM, Fidel S, et al. Impact of needle insertion depth on the removal of hard-tissue debris. Int Endod J. 2017;50(6):560-568. doi:10.1111/iej.12648

3.Narasimhan B, Vinothkumar TS, Praveen R, Setzer FC, Nagendrababu V. A Modified Partial Platform Technique to Retrieve Instrument Fragments from Curved and Narrow Canals: A Report of 2 Cases. J Endod. 2021;47(10):1657-1663. doi:10.1016/j.joen.2021.07.009

4.Setzer FC, Böhme CP. Influence of combined cyclic fatigue and torsional stress on the fracture point of nickel-titanium rotary instruments. J Endod. 2013;39(1):133-137.

doi:10.1016/j.joen.2012.10.001

5.da Frota MF, Espir CG, Berbert FLCVC V, Marques AAFF, Sponchiado-Junior EC, Tanomaru-Filho M, et al. Comparison of cyclic fatigue and torsional resistance in reciprocating single-file systems and continuous rotary instrumentation systems. J Oral Sci. 2014;56(4):269-275. doi:10.2334/josnusd.56.269

6.Klymus ME, Alcalde MP, Vivan RR, Só MVR, de Vasconselos BC, Duarte MAH. Effect of temperature on the cyclic fatigue resistance of thermally treated reciprocating instruments. Clin Oral Investig. 2019;23(7):3047-3052.

doi:10.1007/s00784-018-2718-1

7.da Silva Limoeiro AG, Dos Santos AHB, De Martin AS, Kato AS, Fontana CE, Gavini G, et al. Micro-Computed Tomographic Evaluation of 2 Nickel-Titanium Instrument Systems in Shaping

Root Canals. J Endod. 2016;42(3):496-499. doi:10.1016/j.joen.2015.12.007

8.Rodrigues CT, Duarte MAH, de Almeida MM, de Andrade FB, Bernardineli N. Efficacy of CM-Wire, M-Wire, and Nickel-Titanium Instruments for Removing Filling Material from Curved Root Canals: A Micro-Computed Tomography Study. J Endod. 2016;42(11):1651-1655. doi:10.1016/j.joen.2016.08.012

9.Pinheiro SR, Alcalde MP, Vivacqua-Gomes N, Bramante CM, Vivan RR, Duarte MAHH, et al. Evaluation of apical transportation and centring ability of five thermally treated NiTi rotary systems. Int Endod J. 2018;51(6):705-713.

doi:10.1111/iej.12881

10.]Ehrhardt IC, Zuolo ML, Cunha RS, De Martin AS, Kherlakian D, De Carvalho MCC, et al. Assessment of the separation incidence of mtwo files used with preflaring: prospective clinical study. J Endod. 2012;38(8):1078-1081.

doi:10.1016/j.joen.2012.05.001

11.Bahia MGA, Melo MCC, Buono VTL. Influence of simulated clinical use on the torsional behavior of nickel-titanium rotary endodontic instruments. Oral Surg Oral Med Oral Pathol Oral Radiol Endod. 2006;101(5):675-680.

doi:10.1016/j.tripleo.2005.04.019

12.Alcalde MP, Tanomaru-Filho M, Bramante CM, Duarte MAH, Guerreiro-Tanomaru JM, Camilo-Pinto J, et al. Cyclic and Torsional Fatigue Resistance of Reciprocating Single Files Manufactured by Different Nickel-titanium Alloys. J Endod. 2017;43(7):1186-1191.

doi:10.1016/j.joen.2017.03.008

13.de Menezes SEAC, Batista SM, Lira JOP, de Melo Monteiro GQ. Cyclic Fatigue Resistance of WaveOne Gold, ProDesign R and ProDesign Logic Files in Curved Canals In Vitro. Iran Endod J. 2017;12(4):468-473. doi:10.22037/iej.v12i4.17494

14. Stringheta CP, Pelegrine RA, Kato AS, Freire LG, Iglecias EF, Gavini G, et al. Micro-computed Tomography versus the Cross-sectioning Method

to Evaluate Dentin Defects Induced by Different Mechanized Instrumentation Techniques. J Endod. 2017;43(12):2102-2107.

doi:10.1016/j.joen.2017.07.015

15.Macedo FPG, Soares A de J, Marceliano-Alves MFV, Martinez E, Lopes R, Bastos LF, et al. The effect of root canal preparation tapers on planktonic bacteria and biofilm reduction in the apical third: A correlative microtomography and microbiological laboratory study. Int Endod J. 2024;57(6):700-712. doi:10.1111/jej.14052

16.Al-Nasrawi SJH, Ayad Jaber Z, Talib Al-Quraine N, Imhemed Aljdaimi A, Jabbar Abdul-Zahra Al-Hmedat S, Zidan S, et al. Impact of Peracetic Acid on the Dynamic Cyclic Fatigue of Heat-Treated Nickel-Titanium Rotary Endodontic Instrument. Int J Dent. 2021;2021:6676005.

doi:10.1155/2021/6676005

17.Marim AZ, Bueno CE da S, Stringheta CP, Pelegrine RA, De Martin AS, Rocha DGP, et al. In vitro study of structural and chemical changes in two reciprocating files after multiple reuses and sterilisation. Australian Endodontic Journal. 2024;(November 2023):1-11.

doi:10.1111/aej.12861

18.Moraes RDR, Santos TMP Dos, Marceliano-Alves MF, Pintor AVB, Lopes RT, Primo LG, et al. Reciprocating instrumentation in a maxillary primary central incisor: A protocol tested in a 3D printed prototype. Int J Paediatr Dent. 2019;29(1):50-57. doi:10.1111/ipd.12429

19.Caviedes-Bucheli J, Rios-Osorio N, Usme D, Jimenez C, Pinzon A, Rincón J, et al. Three-dimensional analysis of the root canal preparation with Reciproc Blue®, WaveOne Gold® and XP EndoShaper®: a new method in vivo. BMC Oral Health. 2021;21(1):88. doi:10.1186/s12903-021-01450-1

20. Ordinola-Zapata R, Crepps JT, Arias A, Lin F. In vitro apical pressure created by 2 irrigation needles and a multisonic system in mandibular molars. Restor Dent Endod. 2021;46(1):e14.

doi:10.5395/rde.2021.46.e14

21. Tanomaru AA, Limoeiro AG, de Jesus Soares A, Junior ELM, Campos GR, Hamasaki SK, et al. Influence of Sodium Hypochlorite and Chlorhexidine on the Dynamic Cyclic Fatigue Resistance of XP Endo Shaper Instruments. Eur J Dent. 2022;16(3):580-584. doi:10.1055/s-0041-1735934

22.Kwak SW, Ha JHH, Shen Y, Haapasalo M, Kim HCC. Comparison of the effects from coronal preflaring and glide-path preparation on torque generation during root canal shaping procedure. Aust Endod J. 2022;48(1):131-137.

doi:10.1111/aej.12548

23.La Rosa GRM, Shumakova V, Isola G, Indelicato F, Bugea C, Pedullà E. Evaluation of the cyclic fatigue of two single files at body and room temperature with different radii of curvature. Materials. 2021;14(9):2-9.

doi:10.3390/ma14092256

24. Huang X, Shen Y, Wei X, Haapasalo M. Fatigue Resistance of Nickel-titanium Instruments Exposed to High-concentration Hypochlorite. J Endod. 2017;43(11):1847-1851.

doi:10.1016/j.joen.2017.06.033

25. Nogueira D, Bueno CEDS, Kato AS, Martin AS De, Pelegrine RA, Limoeiro AGDS, et al. Effect of immersion in sodium hypochlorite on the cyclic fatigue resistance of three rotary instruments. J Conserv Dent. 2020;23(6):554-557.

doi:10.4103/JCD.JCD_117_19

26.Pedullà E, Grande NM, Plotino G, Pappalardo A, Rapisarda E. Cyclic fatigue resistance of three different nickel-titanium instruments after immersion in sodium hypochlorite. J Endod. 2011;37(8):1139-1142.

doi:10.1016/j.joen.2011.04.008

27.Mandel E, Adib-Yazdi M, Benhamou LM, Lachkar T, Mesgouez C, Sobel M. Rotary Ni-Ti profile systems for preparing curved canals in resin blocks: influence of operator on instrument breakage. Int Endod J. 1999;32(6):436-443. doi:10.1046/j.1365-2591.1999.00239.x

28.Basturk FB, Özyürek T, Uslu G, Gündoğar M. Mechanical Properties of the New Generation RACE EVO and R-Motion Nickel-Titanium Instruments. Materials (Basel). 2022;15(9). doi:10.3390/ma15093330

29.Bürklein S, Maßmann P, Schäfer E, Donnermeyer D. Cyclic Fatigue of Different Reciprocating Endodontic Instruments Using Matching Artificial Root Canals at Body Temperature In Vitro. Materials. 2024;17(4). doi:10.3390/ma17040827

30.Maniglia-Ferreira C, de Almeida Gomes F, Ximenes T, Neto MAT, Arruda TE, Ribamar GG, et al. Influence of reuse and cervical preflaring on the fracture strength of reciprocating instruments. Eur J Dent. 2017;11(1):41-47. doi:10.4103/ejd.ejd_272_16

31.Ounsi HF, Salameh Z, Al-Shalan T, Ferrari M, Grandini S, Pashley DH, et al. Effect of clinical use on the cyclic fatigue resistance of ProTaper nickeltitanium rotary instruments. J Endod. 2007;33(6):737-741.

doi:10.1016/j.joen.2007.03.006

Influence of cervical and middle preparation on the cyclic fatigue resistance of Logic 25.06 rotary instruments: Replica study.			